

Jenan S. Kashan Biomedical Engineering
Department, University of
Technology, Baghdad, Iraq
70010@uotechnology.edu.iqReceived on: 05/11/2018
Accepted on: 27/02/2019
Published online: 25/05/2019

Optimization Using Taguchi Method for Physical and Mechanical Properties of Bio Mimicking Polymeric Matrix Composite for Orthodontic Application

Abstract- This work take in consideration the application of Taguchi optimization methodology in optimizing the parameters for processing (composition, compounding pressure) and their effects on the output physical (Density and true porosity) properties and mechanical(fracture strength and microhardness) properties for the Nano HA,Al₂O₃ fillers reinforced HDPE hybrid composite material for orthodontic application. An orthogonal array of the Taguchi approach was used to analyses the effect of the processing parameters on the physical and mechanical properties. On the other hand, the surface roughness and particle size distribution were also calculated to study their effect on the output properties. The result shows that the Taguchi approach can determine the best combination of processing parameters that can provide the optimal physical and mechanical conditions, which are the optimum values (the optimum composition was 15HA/ 5Al₂O₃/80HDPE, and optimum compounding pressure was 102 MPa.

Keywords- Taguchi method, Physical Properties , hybrid biocomposite, Mechanical properties

How to cite this article: J.S. Kashan, "Optimization Using Taguchi Method for Physical and Mechanical Properties of Bio Mimicking Polymeric Matrix Composite for Orthodontic Application," *Engineering and Technology Journal*, Vol. 37, Part A, No. 5, pp. 181-187, 2019.

1. Introduction

The fracture, damage, and disease consider the main causes for argent need to use natural or synthetic origin tissue for replacements or repair for the damaged bone. Rapidly growth in population and argent needs for using natural bone grafts make the situation even worse; therefore, there is a high clinical demand for bone substitutes [1]. The xenografts are generally led to viral infections. On the other hand, there is also many limitations for human allografts [2] because there are many risks of transmitting tumor cells, and a variety of bacterial and viral infections [3-6].

Auto grafts conceders the best solution among any substitution materials, because they are osteogenic, osteoinductive, osteoconductive, very biocompatible, non-toxic and non-allergenic [7,8]. Reinforcing polymer with Nano sized ceramics particles is considered high potential materials with enhanced performance without recourse to expensive synthesis procedures [9]. Among many types of Nano ceramics fillers, bioactive ceramics like hydroxyapatite, which is considered the most important substitution materials due to the similarity with a mineral component in the natural bone. While HDPE polymer consider the most suitable replacement for natural collagen in the natural bone.

Therefore, many previous studies proposed [10-13]. HA/HDPE composite as most potential biocomposite for natural bone replacement. The limitation of using HA/HDPE bio composite was due to fragile mechanical properties so that its clinical application was limited to bones with low load bearing strength such as middle ear or orbital floor implants [14]. The mechanical properties of alumina and it's in vivo stability have made it a good alternative in total hip replacement (THR) for some time, Abrasion resistance, strength and chemical inertness of alumina have made it be recognized as a ceramic for dental and bone implants [15,16]. This study is suggesting more than one approaches to develop hybrid Nano bio system for bone replacement. First, the effect of using Nano-sized HA and their effect of the behavior of the biocomposite, secondly, using more than one nano filler to improve mechanical properties for the proposed system and finally using hot pressing technique instead of twin screw extruder (which is mainly used) to fabricate the samples and study its effect on the mechanical properties for the hybrid nano biocomposite.

2. Materials and Methods

I. Materials

Hydroxyapatite powder of 99% purity with an average particle size of 20 nm and a nodular shape and Al₂O₃ powder with an average particle size of 20 nm having a spherical shape were supplied by M.K. Nano (Toronto, Canada) has been used in this study. HDPE powder with a particle size of 5 μm supplied by Right Fortune Industrial Limited (Shanghai, China) was used as a matrix for the composite material.

II. Composite fabrication

Hot pressing technique is considered a high potential technique to produce hybrid polymeric matrix composite due to homogenous distribution of load within the powdered samples, tensile machine was used to apply the load uniformly with double action, while tool steel die with four surrounding heaters was used to prepare disk-shaped samples with diameters of 10 mm and high between 6-8 mm.

The heaters were connected to digital heat controller to manage the hot pressing technique. Four loads of 85, 92, 98 and 102 were used. Hot pressing took place at 130-°C temperature.

III. Density and Porosity measurements

Apparent porosity for the samples has been calculated using the Archimedes method. Which is based on soaking the samples in kerosene for 2h in an evacuated desiccator. The weight of saturated sample suspended in kerosene (W_i) and its weight in the air, after removal of kerosene film from the outer surface, (W_s) were recorded, while W is the dry samples' weight.

Apparent porosity (P) is measured according to the following equation [17]:

$$P = \frac{W_s - W}{W_s - W_i} \times 100\% \quad (1)$$

Bulk density for all samples was measured using a pycnometer instrument of type AccuPyc1330 Pycnometer (AccuPyc from Micromeritics Instrument Corporation, Holland).

Sample testing Procedures [18]:

1. Drying the samples in the oven at a temperature of 60 °C for 48 hr. to remove moisture.
2. Weighting the samples using 4 digit balances.
3. Loading the sample into the pycnometer cell, and sealing it carefully.
4. Opening the helium gas valve and programming the instrument to start the analysis.

IV. Mechanical Testing

Microhardness tester (Digital Micro-Vickers Hardness tester TH714) for Beijing TIME High Technology Ltd./China) was used at a load of 75gm and testing time 10sec to measure the microhardness for all samples.

While the diametrical compression test was used to measure the fracture strength for all samples. This test is used for materials which are too difficult to process or machine into the ASTM standard "dogbone" shaped specimen, which is pulled in tension[19],[20]

Fracture strength can be measured using the following equation [19]:

$$\sigma_f = 2P/\pi Dt \quad (2)$$

Where:

σ_f : Tensile fracture strength (MPa), P: Cross head load (N), D: Specimen diameter (mm)

t: Specimen thickness(mm).

V. Particle Size and Particle Size Distribution measurements

Master sizer 2000 was used to measure the particle size and particle size distribution for samples after hot pressing took place. The Mastersizer 2000 uses the technique of laser diffraction to measure particle size distributions from 10nm up to 3.5mm [21]. The powder agglomerates size and distribution is considered a very important factor which has a direct effect on the biological behavior of the biomaterials implant within the human body. Because it controls the porosity size and shape, which have a great impact on the osteoinduction and osteointegration process.

VI. Optimization using Taguchi approach

During the fabrication of biomaterials, many experiments maybe take place to evaluate similar bio mimicking properties that should be similar to the natural living tissues. So that optimization process is considering a very helpful tool to minimize the number of experiments that should be done to produce suitable biomaterials. Taguchi method is considered very helpful tool for the design of experiments based on the number of factors and control levels [22,23].

3. Results and Discussion

I. Density and Porosity

Figure (1a) shows the effect of compounding pressure on the measured bulk density, while Figure (1b) shows the effect of this factor on the apparent porosity. Both Figures compared the previous values at different compositions.

The measured values of density seems to increase with maximizing the pressure, this maybe attributes to the densification process due to increase the contact surfaces between nano and micro particles which increase the mechanical bonding between particles, furthermore, while heating process the storage energy during pressing process transform to activation energy for chemical bonding and reduce the pores amount and size of the porosity which is very noticeable in Figure 1b.

The porosity values increased with increasing the filler volume fraction because the Nano particles tends to coat the polymer micron-sized particles during dry mixing process and this effect creates a micro-sized agglomerates which will cause and increasing in porosity value, in the same time the porosity values decreased with increasing the compacting pressure because the pressure decreases the spaces between particles [24].

II. Mechanical Properties

The effect of compression pressure and the filler volume fraction on the mechanical properties are shown in Figure 2. For the Nano HA/HDPE composite samples, the values of micro-hardness and fracture strength increase with increasing the compressive pressure due to interconnection and bonding between the filler and the polymer matrix which increase with increasing the pressure.

For the HA/Al₂O₃/HDPE composite system, a significant enhancement in hardness values has been recognized, which can be attributed to the Alumina mechanical properties [25,26].

III. Particle size and particle size distribution

Particle size and particle size distribution took place for the samples after hot pressing; the samples were randomly braked and crashed, the resulted powder was charged to the mastersizer machine. This step considering very important because it gives a strong indication about the biological response for the bio composite when implanted in the living tissue, especially the osteoinduction and proliferation process.

According to previous literature [27,28], the best properties wrer established at 20 and 40 vol% HA so that we select 40 vol% HA/HDPE samples for this test. Figure 3a shows the particle size distribution for 40HA/60HDPE sample, and Figure 3b shows the same measurements for the 40HA/5Al₂O₃/HDPE because they reflect the best properties for the proposed biocomposite.

These results are showing that the biocomposite with alumina content has finest agglomeration size with uniform distribution, this maybe attributes to the existence of more than one Nano filler which tends to create smaller agglomerates than HA/HDPE composite because of dynamic coating between Nano and micro components [29].

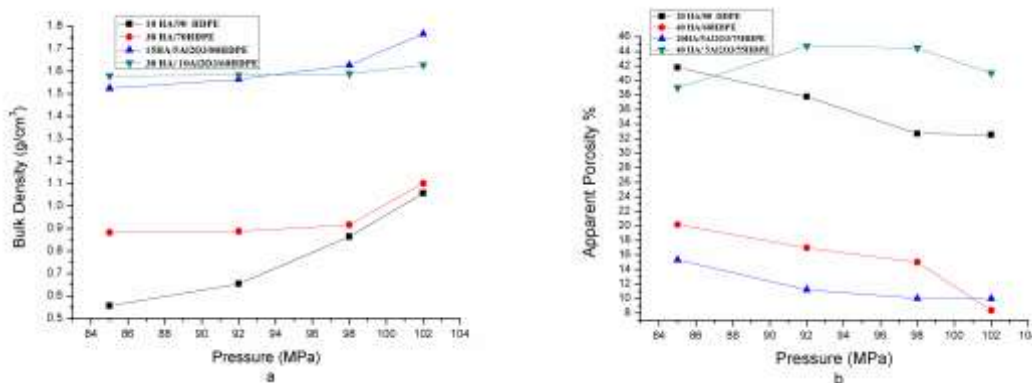


Figure 1: a) Effect of pressure on the bulk density, b) Effect of pressure on the apparent porosity.

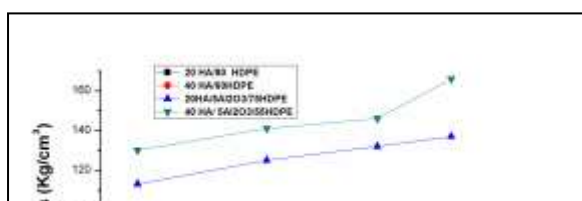
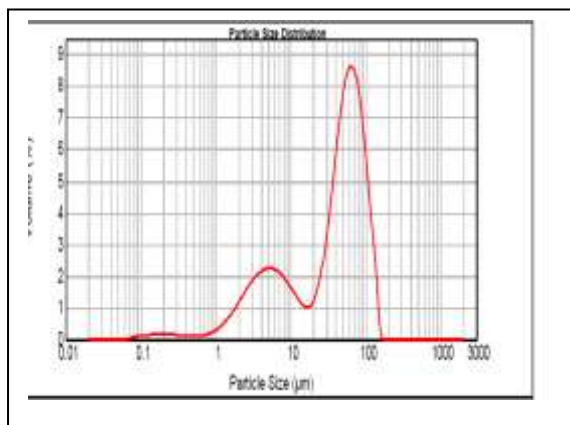
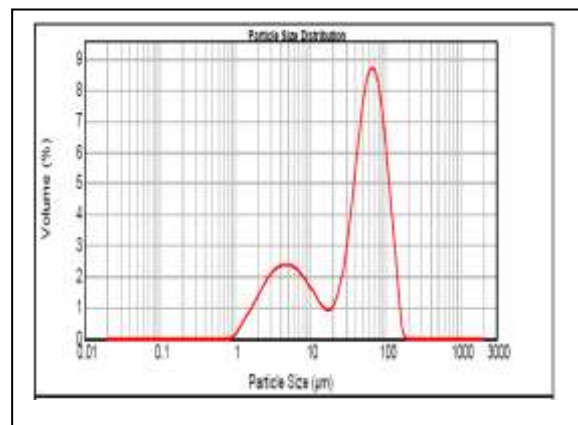


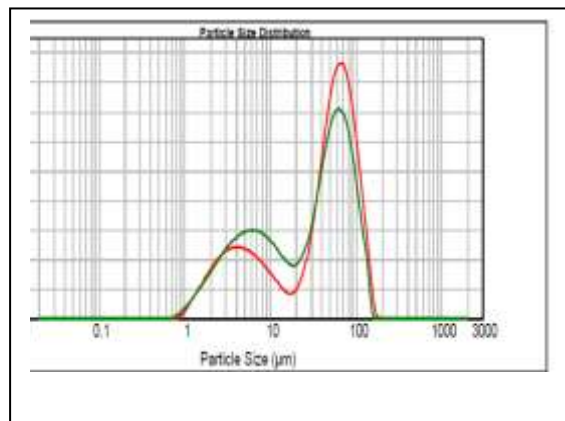
Figure 2: a) Effect of pressure on the microhardness, b) Effect of pressure on the fracture strength



a



b



c

Figure 3: a) Particle size in µm size and Particles distribution for 40 vol% HA/HDPE samples, b) for 40HA/5Al₂O₃/HDPE, c) Mixed run.

IV. Determination of the optimum processing parameter

1. Density

The-larger-the-better has applied to examine the highest bulk density that could be the best condition for this study. The charts in Figure 4 are used to determine the optimal set of parameters. From these charts, the control factor of composition (A) at level 1 (20 HA/80 HDPE) gave the optimum result. While the compression pressure control factor (B) gave the optimum result at level 4 (102 MPa). Table 1 shows the analysis results for density. Because of the input parameters (composition and pressure), the S/N ratio is very small and maybe neglected for all measurements.

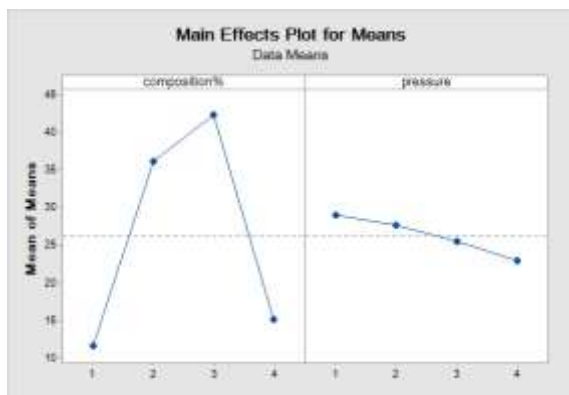


Figure 4: Taguchi Analysis: Density versus composition %; pressure.

Table 1: Response Table for Means: Density

Level	Composition%	Pressure
1	1.6203	1.1352
2	0.7827	1.1717
3	1.5942	1.2490
4	0.9465	1.3878
Delta	0.8375	0.2525
Rank	1	2

2. Fracture strength

The-larger-the-best criteria used to determine the highest fracture strength that could be the best condition for this study. The charts in Fig. 5 are used to determine the optimum set of parameters. From these charts, the control factor of composition (A) at level 1 (20 HA/80 HDPE) gave the optimum result. While the compression pressure control factor (B) gave the optimum result at level 4 (102 MPa). Table 2 shows the analysis results for fracture strength.

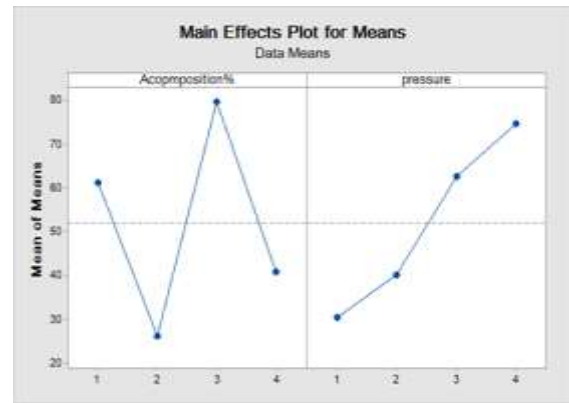


Figure 5: Taguchi Analysis: Fracture strength versus composition %; pressure.

Table 2: Response Table for Means: Fracture strength

Level	Composition%	Pressure
1	61.25	30.50
2	26.25	40.25
3	79.75	62.75
4	41.00	74.75
Delta	0.2525	53.50

3. Microhardness

From Figure 6, the control factor of composition (A) at level 3 (15HA/ 5Al₂O₃/80HDPE) gave the optimum result. While the compression pressure control factor (B) gave the optimum result at level 4 (102 MPa). Table 3 show the analysis results for microhardness.

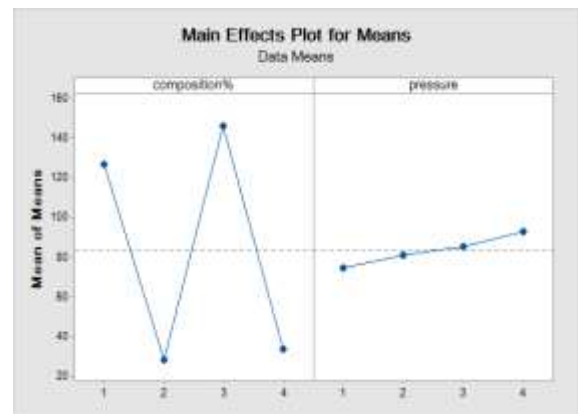


Figure 6: Taguchi Analysis: Microhardness versus composition %; pressure

Table 3: Response Table for Means: Microhardness

Level	Composition%	Pressure
1	126.75	74.75
2	28.50	81.25
3	145.75	85.50
4	33.50	93.00
Delta	117.25	18.25

4. Porosity

The -larger-the-better characteristic was used to determine the maximum that would be the ideal situation for this study because the porosity is concenter the key factor in the producing of biomaterials for bone substitute application. The charts in Figure 7 are using to determine the optimum set of parameters in case of maximum values. From these charts, the control factor of composition (A) at level 3 (15HA/5Al2O3/80HDPE) gave the optimum result. While, the compression pressure control factor (B) gave the best result at the level 1 (85 MPa). Table 4 show the analysis results for true porosity.

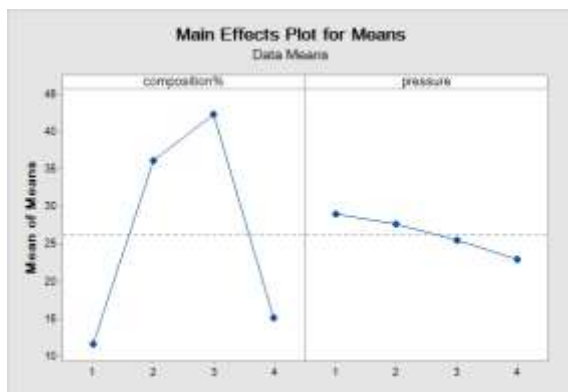


Figure 7 Taguchi Analysis: Max Porosity versus composition%; pressure

Table 4: Response Table for Means: Max Porosity

Level	Composition%	Pressure
1	11.64	29.07
2	36.20	27.68
3	42.30	25.54
4	15.14	22.98
Delta	30.66	6.09
Rank	1	2

4. Conclusion

In present work, the Taguchi method used to select the optimum possessing as an approach to finding the best-resulted properties for the proposed bio composite system from varying combinations of compression pressures and compositions. A basic level was 3 in most cases so that, the optimized values were similar to the measured values so that this optimizing method concenter very effective way to determine the optimum processing parameters to reach best properties for the proposed bio composite

References

[1] J. Keating, M.McQueen “Substitutes for autologous bone graft in orthopedic trauma,” J Bone Joint Surg Br, 82, 3-8, 2001.

[2] A. Chau, R. Mobbs “Bone graft substitutes in anterior cervical discectomy and fusion,” Eur Spine J, 18, 449-64, 2009.

[3] K. Kaveh, R. Ibrahim, M. Bakar, T. Ibrahim, “Bone grafting and bone graft substitutes,” J Anim Vet Adv, 9, 1055-67, 2010.

[4] R. Murugan, S.Ramakrishna “Bioactive nanomaterials in bone grafting and tissue engineering,” In: Handbook of nanostructured biomaterials and their applications in nanobiotechnology, Nalwa HS (Ed.); American Scientific Publishers: Stevenson Ranch USA, 2, 141-8, 2005.

[5] J. Tazaki, M. Murata, T. Yuasa, T. Akazawa, K. Ito, J. Hino, “Autograft of human tooth and demineralized dentin matrices for bone augmentation,” J Ceram Soc Jpn, 118, 442-5, 2010.

[6] J. Conway, “Autograft and nonunions: morbidity with intramedullary bone graft versus iliac crest bone graft,” Orthop Clin North Am, 41, 75-84, 2010.

[7] E. Keller, W. Triplett “Iliac crest bone grafting: review of 160 consecutive cases,” J Oral Maxillofac Surg, 45, 11-4, 1987.

[8] A.D. Thamir, J.S. Kashan, J.T.Alhaidary, “Effect of Particle Size on the Physical and Mechanical Properties of Nano HA/HDPE Bio-Composite for Synthetic Bone Substitute,” Eng. & Tech. Journal, Vol. 32, Part (A), No.2, 2014.

[9] E. Tolba, B.M. Abd-Elhady, B. Elkholy, H. Elkady, “Biomimetic Synthesis of Guided-Tissue Regeneration Hydroxyapatite/Polyvinl Alcohol Nanocomposite Scaffolds: Influence of Alignate on Mechanical and Biological Properties,” J. Americ. Scie, 6,196, 2010.

[10] M. Wang, W. Bonfield, “Chemically coupled hydroxyapatite- polyethylene composites: structure and properties,” J. Biomater, 22, 1311, 2001.

[11] R.A. Sousa, R.L. Reis, A.M. Cunha, M.J. Bevies, “Coupling of HDPE/hydroxyapatite Composite by Silane-based Methodologies,” J. Mater. Sci. Mater. In Medicine, 14, 475, 2003.

[12] R. L. Reis, A. M. Cunha, M.J. Oliveira, A.R. Campos, M.J. Bevis, “Relationship between processing and mechanical properties of injection molded high molecular mass polyethylene + hydroxyapatite composites,” J. Mat Res Innovat ,4, 263, 2001.

[13] S. Kangwantrakool, “Preparation of Hydroxyapatite-Polyethylene Biocomposites Using HA-nanoparticles by Mechanically-Coating Method,” CMU Journal Special Issue on Nanotechnology, 4, 95, 2005.

[14] M. Haneef, J. Rahman, M. Yunus, S. Zameer, S. Patil, T. Yezdani, “Hybrid Polymer Matrix Composites for Biomedical Applications,” IJMER, 3:2, pp-970-979, 2013.

[15] A. Tathe, M. Ghodke, A. Pratima, A. Nikalje, “Brief review on biomaterials and their applications,” International Journal of Pharmacy and Pharmaceutical Sciences, Volume 2, Suppl 4 , pp 19-23, 2010.

[16] J. Black, G. Hasting “Handbook of biomaterials Properties,” London, UK: Chapman Hall, 1998.

- [17] E. Tolba, B.M. Abd-Elhady, B. Elkholy, H. Elkady, "Biomimetic Synthesis of Guided-Tissue Regeneration Hydroxyapatite/Polyvinyl Alcohol Nanocomposite Scaffolds, Influence of Alignate on Mechanical and Biological Properties," *J. Americ. Scie*, 6,196, 2010.
- [18] AccuPyc 1330 Pycnometer Operator's Manual V3.03, Micromeritics Instrument Corporation, 2001.
- [19] L. WANG, P. Henrique P. D'alipino, L.G. Lopes, J.C. Perira, "Mechanical Properties of Dental Restorative Materials: Relative Contribution of Laboratory tests, *J. Appl. Oral Sci*, 11,162, 2003.
- [20] A.T. Procopio, A. Zavaliangos, J.C. Cunningham "Analysis of the diametrical compression test and the applicability to plastically deforming materials," *J. Mater. Sci.*, 38, 3629, 2003.
- [21] www.malvern.com, Mastersizer Manual, Malvern Instruments Limited Grovewood Road, Malvern, Worcestershire, UK, WR14 1XZ.
- [22] S.S. Mahapatra, A. Patnaik, "Study on mechanical and erosion wear behavior of hybrid composites using Taguchi experimental design," *Mater. Des.* 30, 2791–2801, 2009.
- [23] P. Ross, "Taguchi Techniques for Quality Engineering: Loss Function, Orthogonal Experiments, Parameter and Tolerance Design," McGraw-Hill, New York, 1998.
- [24] T. Thamaraiselvi, S. Rajeswari, "Biological Evaluation of Bioceramic Materials - A Review," *Trends Biomater. Artif. Organs*, 18, 1, pp 9-17, 2004.
- [25] V. Sergey "Biocomposites and hybrid biomaterials based on calcium orthophosphates," *Biomatter* 1, 1, 3-56, 2011.
- [26] T. Kokubo, H. Kim, M. Kawashita "Novel bioactive materials with different mechanical properties," *Biomaterials*, 24, 2161-75, 2003.
- [27] J.S. Kashan, A. Jha, A.D. Thamir, J.T. Al-Haidar, "A kinetic analysis of the melting HA/Y-PSZ/HDPE nano composite for hard tissue materials," *Journal of King Saud University – Engineering Sciences*, 30, 286–29, 2018.
- [28] J.S. Kashan, H. Jameel, "The Development of Biomimetic Nano CaCO₃/ PPBio Composites as Bone Repair Materials- Optimal Thermal Properties Evaluation," *J. of Babylon Univ ersity/Engineering Sciences*, No. 5, Vol. 25, 1562-1571, 2017.
- [29] J.S. Kashan, A.D. Thamir, J.T. Al-Haidary, "Effect of Particle Size on the Physical and Mechanical Properties of Nano HA/HDPE Bio-Composite for Synthetic Bone Substitute," *Eng. & Tech. Journal*, Vol.32, Part (A), No.2, 286-297, 2014.